## Modelling Drug Release from a Polymer

Shaunagh Downing, Sinead Finn, Amy Joyce, Ciaran McDonnell

Stokes Modelling Workshop National University of Ireland,Galway

June 18, 2015

イロト イポト イヨト イヨト

**Problem Description** 

Formulating the Problem

Solving the Problem

Applications

Conclusions

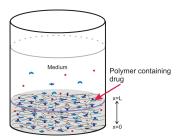
・ロン ・回と ・ヨン・

æ

# Problem Description

#### Task:

To model the diffusion of a drug from a polymeric wafer to a release medium, considering the effect of geometry on the rate of diffusion.





### Assumptions

- Planar System
- Diffusion through one surface only
- Initial uniform concentration of the drug in the polymer

イロト イヨト イヨト イヨト

- The release medium is a perfect sink
- Constant diffusion coefficient

# **Dimensional Analysis**

Through Dimensional analysis and the Buckingham Pi theorem, the reduced formula for the time it takes half the drug to be released was found to be

$$\tau_{\frac{1}{2}} = \frac{H^2}{D} G\left(c_0 H^3\right)$$

イロト イポト イヨト イヨト

where  $G(c_0H^3)$  is a function of the initial concentration and position of the drug.

### **Diffusion Equation**

$$\frac{\partial c}{\partial t} = D \frac{\partial^2 c}{\partial x^2}$$

・ロン ・回と ・ヨン・

æ

Where:

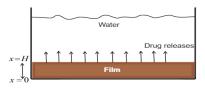
$$c = c(x,t) = concentration of drug in polymer$$

t = time

x = position

D = Diffusion Coefficient (constant)

## Boundary and Initial Conditions



The polymer occupies 0 < x < HBoundary Conditions

c = 0 on x = H, t > 0 (perfect sink condition)

$$\frac{\partial c}{\partial x} = 0$$
, on  $x = 0, t > 0$  (no flow condition)

### **Initial Conditions**

 $c = c_0, 0 < x < H, t = 0$  , (3) (3) (3)

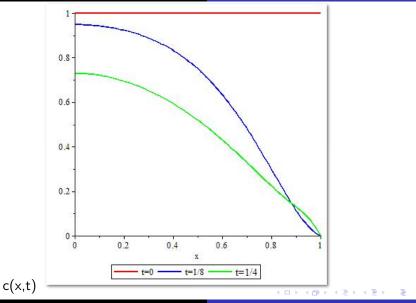
# PDE Solution

The initial boundary value problem was solved through separation of variables. The concentration was found to be:

$$c(x,t) = \sum_{n=0}^{\infty} \left[ \left( \frac{c_0 \left( -1 \right)^n}{\left( n + \frac{1}{2} \right) \pi} \right) cos \left( \frac{\left( n + \frac{1}{2} \right) \pi x}{H} \right) e^{\frac{-\left( n + \frac{1}{2} \right) \pi^2 D t}{H^2}} \right]$$

イロト イヨト イヨト イヨト

æ



M(t) is defined as the amount of drug diffused from the polymer into the release medium, that is: (the total amount of drug) - (the amount of drug left in the

polymer at time t)

$$M(t) = AHc_0 - \int_0^H Ac(x, t) dx$$

which is calculated to be:

$$M(t) = AHc_0 \left[ 1 - \frac{2}{\pi^2} \sum_{n=0}^{\infty} \left( \frac{1}{\left(n + \frac{1}{2}\right)^2} \right) e^{\frac{-\left(n + \frac{1}{2}\right)\pi^2 D t}{H^2}} \right]$$

- 4 同 6 4 日 6 4 日 6

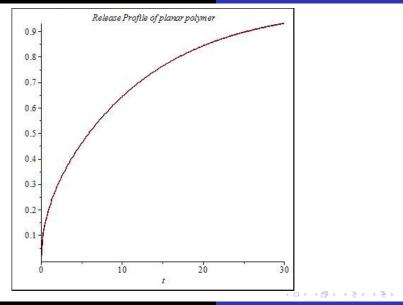
#### **Release Profile**

The release profile is a plot of  $\frac{M(t)}{M(\infty)}$  against time. For the planar release profile:

$$\frac{M(t)}{M(\infty)} = \left[1 - \frac{2}{\pi^2} \sum_{n=0}^{\infty} \left(\frac{1}{\left(n + \frac{1}{2}\right)^2}\right) e^{\frac{-\left(n + \frac{1}{2}\right)\pi^2 D t}{H^2}}\right]$$

・ロン ・回と ・ヨン・

æ



Shaunagh Downing, Sinead Finn, Amy Joyce, Ciaran McDonne Modelling Drug Release from a Polymer

æ

Using the expression for  $\frac{M(t)}{M(\infty)}$ , then

$$\frac{M\left(\tau_{\frac{1}{2}}\right)}{M(\infty)} = 1 - \frac{2}{\pi^2} \sum_{n=0}^{\infty} \left(\frac{1}{\left(n + \frac{1}{2}\right)^2}\right) e^{\frac{-\left(n + \frac{1}{2}\right)^2 \pi^2 \tau_{1/2}}{H^2}} = \frac{1}{2}$$

Solving numerically for  $\tau_{\frac{1}{2}}$ :

$$au_{rac{1}{2}} = 0.197 rac{H^2}{D}$$

・ロン ・回 と ・ ヨ と ・ ヨ と

3

 $\therefore G(H^3c_0)$  is a constant.

 $\implies$  The timescale over which the drug releases has no dependance on initial concentration  $c_0$ .

A parameter regime can be designed for the release of the drug over specific time intervals. For a H of 2mm:

- 1 day:  $D = 4.00 \times 10^{-6} m^2 / day$
- 1 week:  $D = 5.71 \times 10^{-7} m^2 / day$
- **1** month:  $D = 1.33 \times 10^{-7} m^2 / day$

- 4 同 6 4 日 6 4 日 6

### Geometries

A similar analysis can be made to find the release profiles for polymers of different geometries.

### Spherical

$$\frac{M(t)}{M(\infty)} = 1 - \frac{6}{\pi^2} \sum_{n=1}^{\infty} \left( \frac{(-1)^{n+1}}{n^2} \right) e^{-\frac{Dn^2 \pi^2 t}{R^2}}$$

### Cube

$$\frac{M(t)}{M(\infty)} = 1 - \frac{8}{\pi^6} \sum_{n,m,p=1}^{\infty} \left[ \frac{(1 - (-1)^n)^2 (1 - (-1)^m)^2 (1 - (-1)^p)^2}{(nmp)^2} \right]$$
$$x \left( e^{-\frac{D\pi^2 (n^2 + m^2 + p^2)t}{R^2}} \right)$$

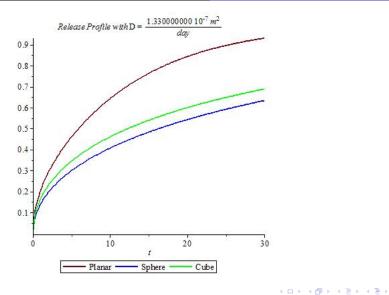
### Cylindrical

$$\frac{M(t)}{M(\infty)} = 1 - \frac{32}{\pi^2} \left( \sum_{n=1}^{\infty} \frac{1}{q_n^2} e^{\frac{-q_n^2}{R^2} Dt} x \sum_{p=0}^{\infty} \frac{1}{(2p+1)^2} e^{\frac{-(2p+1)^2}{H^2} \pi^2 Dt} \right)$$

Where  $q_n$  are the roots of the Bessel function of the first kind of zero order.

イロン イヨン イヨン イヨン

æ



Shaunagh Downing, Sinead Finn, Amy Joyce, Ciaran McDonne Modelling Drug Release from a Polymer

Э

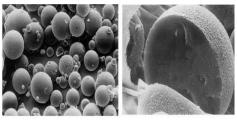




・ロト ・日本 ・モート ・モート

### Planar - Gliadel Wafer

- Localised delivery
- Especailly potent drugs
- Eg. tumour removal



### Spherical - Microsphere

200 µm ------

20 µm ------

イロン イヨン イヨン イヨン

- Long-term sustained release
- Injectable/inhalable
- Ease of mobility through narrow capillaries
- Eg. macular degeneration



- ► The amount of drug released M(t) depends exponentially on thickness H and diffusivity D, and is directly proportional to initial concentration c<sub>0</sub>
- The timescale for drug release is dependant on D and strongly dependant on H. These parameters can be altered during drug manufacture.

イロト イポト イヨト イヨト

- The timescale does not depend on c<sub>0</sub>
- Polymer geometry affects the rate of diffusion of the drug.